Research Article

Design and optimization of mRNAs encoding an Anti-TIGIT antibody with therapeutic potential for cancer in TIGIT-humanized BALB/c Mice

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Abstract

mRNA drugs are synthesized using cell-free systems without complex and stringent manufacturing processes, which makes their preparation simple, efficient, and economical. Over the past few years, mRNAs encoding antibodies have been one of the research frontiers of antibody drug development. In cancer immunotherapy, mRNAs encoding immune checkpoint antibodies may be advantageous regarding antibody persistence and durability of the anti-tumor immune response of patients. In our previous study, a candidate antibody—AET2010—targeting the novel immune checkpoint TIGIT was reported. Its anti-tumor activity was also investigated using adoptive transfer of NK-92MI cells in a xenograft mouse model, but the limitations of the model did not facilitate precise evaluation. In the present study, we further investigated the therapeutic potential of AET2010 for cancer in TIGIT-humanized BALB/c mice. Next, we explored the design, synthesis, and optimization of mRNAs encoding AET2010 and ultimately obtained a candidate mRNA (mRNA-BU) with favorable in vitro and in vivo expression levels of active AET2010. Particularly, lipid-nanoparticle-encapsulated mRNA-BU delivered to mice produced AET2010 with significantly higher peak concentration and expression duration than an equivalent dose of original AET2010. This study provides a sound basis for developing novel drugs targeting TIGIT.

Introduction

Mature mRNAs consist of five structural elements; from 5′ to 3′, these are the cap structure, 5′-untranslated region (UTR), open reading frames (ORFs), 3′ UTR, and poly-A tail (a chain of adenine nucleotides), respectively. The cap structure and poly-A tail protect the mRNA from exonuclease degradation and improve its stability and translation efficiency [1,2]. The UTRs are responsible for regulating translation and protein expression and affect the translation efficiency, half-life, maximum expression level, and stability of the mRNA [3,4]. The translatability of the ORFs is also crucial to the mRNA [5-7]. The in vivo use of in vitro-transcribed (IVT) mRNAs for protein expression dates back to the 1990s [8,9]. A series of design and modification technologies for mRNA synthesis has improved the biological characteristics of IVT mRNAs [1,10,11], thus improving the stability of mRNA molecules and the translation level of proteins. However, mRNAs are negatively charged molecules with a relatively large molecular weight (104–106 Da), which makes it difficult to traverse the anionic lipid bilayer of cells and are easily degraded. Thus, there exist two barriers to mRNA delivery into the cell: enzymatic degradation during delivery and transport across the membrane barrier due to electrostatic repulsion [12]. During the past few years, many innovative solutions based on materials have been developed; the most widely used appears to be the nano-delivery systems. Lipid nanoparticles (LNPs) are biocompatible carriers with...
phospholipid monolayers that encapsulate mRNA, preventing degradation and allowing efficient delivery [13,14]. The gradual resolution of these technical problems makes it possible to synthesize mRNAs in vitro as a therapeutic drug. Specifically, during the coronavirus disease 2019 pandemic, mRNA drug development has been accelerated. The novel coronavirus mRNA vaccine mRNA-1273 developed by Moderna and BNT162b2 jointly developed by Pfizer and BioNTech have been authorized for emergency use, which showed a promising prospect for mRNA drugs [15].

Therapeutic antibodies constitute the primary type of biological drug. However, the complex and stringent manufacturing processes of antibody drug development have hindered patient access to a certain extent. Using mRNA-encoded antibodies may overcome some challenges in the production of antibody drugs. mRNA drugs are biological macromolecules synthesized by a cell-free system and thus do not depend on complex technological processes such as cell culture, scale fermentation, and protein purification, making the production of antibody-encoding mRNAs simple, efficient, and economical [1,16,17]. In addition, in vivo administration of antibody-encoding mRNAs would facilitate the delivery of therapeutic antibodies to the body continuously for a long period, reducing the required frequency of dosing. To date, no drugs consisting of IVT mRNAs encoding antibodies are available in the market; however, significant advances have been made—for example, a successful phase I clinical trial (NCT03829384) of mRNA encoding a neutralizing antibody to Chikungunya virus (CHIKV) has been completed by Moderna [17]. In cancer immunotherapy, treatment with mRNAs encoding immune checkpoint antibodies may be advantageous in terms of antibody persistence and durable anti-tumor immune response of patients.

TIGIT is a novel immune checkpoint molecule expressed in T cells, natural killer (NK) cells, and other immune cells. Its immunomodulatory effects on the function of immune cells make it an attractive candidate drug target. By blocking the signal pathway between TIGIT and its receptors, the exhaustion of tumor-infiltrating NK cells and CD8+ T cells may be reversed, and the anti-tumor immunity of patients may be restored. [18-20]. In a previous study, we obtained a candidate therapeutic antibody—AET2010—targeting TIGIT. The anti-tumor activity of AET2010 was investigated in a xenograft mouse model with an adoptive transfer of NK-92MI cells. However, this model was not sufficient for the precise evaluation of the anti-tumor efficacy of AET2010 because the effect of NK cells was boosted, and the potential anti-tumor effect of CD8+ T cells was overlooked [21].

In the present study, we further investigated and ascertained the therapeutic potential of AET2010 for cancer in TIGIT-humanized BALB/c mice. Subsequently, we explored the design, synthesis, and optimization of mRNAs, and their expression in mice by LNP delivery to obtain a candidate mRNA that could effectively encode AET2010. Totally, our study aimed to provide a sound basis for the development of novel drugs targeting TIGIT.

Materials and methods

Antibody preparation

The genes encoding the variable regions of light and heavy chains of RG6058 (tiraglumab) from patent US10047158B2 were synthesized and cloned into expression vectors pABx and pABg (maintained in our laboratory) respectively. HEK-293F cells were cultured at 37 °C in FreeStyle™293 expression medium (Gibco, NY, USA) and incubated at 37 °C in a 5% CO2 incubator. For antibody expression, Human embryonic kidney 293 cells (HEK-293F) were transfected with equal quantities of heavy chain and light chain expression plasmids using FectoPRO transfection reagent (Polyplus-Transfection SA, FR) and cultured at 37 °C and 5% CO2, while being shaken at 125 rpm for 4 days; the cell cultures were centrifuged at 8000 rpm for 10 min to collect the culture supernatant, which was filtered through a 0.45 µm membrane. Antibodies secreted in the supernatant were purified using HiTrap™ Mabsel ect SuRe™ (Cytiva, 11003493, USA), replacing 0.1 M citric acid buffer (pH 3.0) with phosphate-buffered saline (PBS; pH 7.4) using HiTrap™ desalting columns (Cytiva, 29048684, USA). A spectrophotometer (Thermo Nanodrop One C, NY, USA) was then used to quantify protein concentration, and the presence of the protein was verified by sodium dodecyl sulfate-polyacrylamide gel electrophoresis (SDS-PAGE) analysis.

Surface plasmon resonance assay

The interaction affinity between antibodies and recombinant human TIGIT-His (SinoBiological, Beijing, China) was calculated on the basis of kinetic constants using the BiaCore™ 3000 system. Multi-cycle kinetics analysis was used for kinetic analysis experiments. Purified AET2010, RG6058, and MK7684 (vibostolimab) were captured on a CM5 chip using the Human Antibody Capture Kit (Cytiva, USA). Recombinant human TIGIT-His with a concentration ranging from 2.05 nM to 80.00 nM in HBS-EP+ running buffer was passed over the chip at a rate of 30 μL/min at 25 °C. A 3 min association period was followed by a 6 or 12 min dissociation period. A cycle of repeated measurements was set for quality control, and two cycles of blank controls were used to correct system deviations. The regeneration step consisted of chip flushing with 3 M MgCl2 for 30 s at the rate of 30 μL/min. The experimental data were fit to a 1:1 binding model using BiAcore™ 3000 evaluation software. Equilibrium dissociation constants (Kd) were calculated according to fitting curves.

Mice and animal experiments

Female TIGIT-humanized BALB/c mice (BALB/c-hTIGIT, 6–7 weeks old) were purchased from Gemphtech.
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(T004023, Jiangsu, China). All mice were maintained under specified pathogen-free (SPF) conditions and the animal use protocol was approved by the Animal Ethics Committee of Gempharmatech Co. Ltd. (GPTAP202111203-1). To establish a xenograft tumor model, the mice were subcutaneously inoculated with 100 μL of CT26 colorectal cancer cells suspended in PBS (5 × 10^5 cells per mouse). Tumor dimensions were measured twice weekly, and tumor volume was calculated as follows: volume = 0.5 × long diameter × (short diameter)^2. The mice were randomized into four groups when the tumor volume reached 80–100 mm^3. The day of grouping was defined as D0. On D0, D3, D7, D10, D14 and D17, mice were intraperitoneally injected with AET2010, RG6058, MK7684, and isotype human IgG (10 μg/g of mouse body weight). Mouse body weight and tumor volume were measured at D0, D2, D5, D9, D12, D16 and D19.

Relative tumor volume on day t for mouse number n (RTVn) was calculated as follows:

\[ RTV_n = \frac{V_{nt}}{V_{n0}} \]

Where \( V_n \) indicates tumor volume on day t for mouse number n, and \( V_{n0} \) indicates tumor volume on D0 for mouse number n.

The tumor growth inhibition (TGI) rate was calculated as follows:

\[ TGI = \left( 1 - \left( \frac{\text{mean RTV}_{\text{treat}}}{\text{mean RTV}_{\text{control}}} \right) \right) \times 100\% \]

Where mean RTV_{treat} indicates the mean RTV of a treatment group, and mean RTV_{control} indicates the average RTV of the isotype human IgG group.

**mRNA preparation**

Gene sequences containing the T7 promoter, 5′ UTR, ORF (antibody-coding sequence), and 3′ UTR sequences were synthesized and cloned into pMV plasmid vectors to construct DNA templates. The mRNAs were synthesized in vitro using T7 RNA polymerase-mediated (Vazyme, Nanjing, China) transcription of DNA templates linearized by digestion with XbaI (NEB, USA). Transcribed samples were purified using magnetic beads (Vazyme, Nanjing, China). A 7-methyl guanosine cap (m7Gppp, Cap 0) was added to the 5′ ends of RNA using a vaccinia virus capping system (Vazyme, Nanjing, China), and then the cap was 2′-O-methylated to form Cap 1. The poly-A tail was added to the 3′ UTR using Escherichia coli Poly (A) polymerase (NEB, USA). The prepared mRNAs were verified by agarose gel electrophoresis.

**Cell culture and antibody expression**

Chinese Hamster Ovary cells (CHO) and African green monkey SV40 transformed kidney cells (COS-7) (maintained in our laboratory) were incubated at 37 °C in Dulbecco’s modified Eagle’s minimal essential medium (DMEM) (Procell, Wuhan, China) containing 10% fetal bovine serum (Gibco), 100 U/mL of penicillin, and 100 mg/mL of streptomycin (Gibco). Human Embryonic Kidney 293 Cells (HEK-293F) were incubated at 37 °C in FreeStyle™ 293 expression medium (Gibco).

CHO, COS-7 and HEK-293F cells were seeded in 48-well plates at 100,000 cells/well. After 24 h, cells were transfected with 0.9 μg of mRNA using 2.7 μL of Lipofectamine™ MessengerMAX™ transfection reagent (Thermo Fisher Scientific, MA, USA). The mass ratio of light chain to heavy chain in duplex mRNA was 2:1. The supernatant was collected by centrifuging at 8000 rpm for 10 min at 48 h post-transfection and analyzed by enzymelinked immunosorbent assay (ELISA). The cell cultures were centrifuged at 8000 rpm for 10 min to collect the culture supernatant.

**Enzyme-linked immunosorbent assay**

mRNA-encoded antibody proteins expressed in vitro and in vivo were quantified using ELISA. The concentration of antibody proteins was calculated on the basis of a standard curve. For ELISA, 96-well microplates (Corning, NY, USA) were coated with recombinant human TIGIT-His (prepared in our laboratory; 100 ng per well) and incubated overnight at 4 °C and then blocked with PBS containing 2.5% fat-free powdered milk for 1 h at 37 °C. A standard curve was plotted from serial dilutions (1.465–1000.000 ng/mL) of the original AET2010 in PBS buffer containing 2.5% fat-free powdered milk and 0.1% Tween 20. Cell expression supernatant or mouse serum was serially diluted and then incubated for 1 h at 37 °C. After washing, horseradish peroxidase-conjugated goat anti-human IgG (ZSGB-Bio, Beijing, China) was added to the mixture and incubated for 45 min at 37 °C. The absorbance of the resultant mixture at 450 nm and 595 nm in 3, 3′, 5′-Tetramethylbenzidine (TMB) substrate was measured (Thermo Multiskan MK3).

**Codon optimization**

The distribution of full-length sequence codon usage bias was analyzed using the MinMax% tool [22]. Global codon substitution was performed using the human codon usage bias table (GenBank_63, http://www.kazTsa.or.jp/codon/) and minimum free energy (MFE) of sequences was analyzed using RNA structure (http://rna.urmc.rochester.edu/RNAstructureWeb/) [23,24]. The guanine and cytosine content (GC%) and codon adaptation index (CAI) values were estimated. The secondary structure of mRNA was predicted using LinearDesign Web Server (beta) (http://rna.baidu.com/).

**Lipid nanoparticle formulation**

SM-102, DSPC, cholesterol, and mPEG-DMG-2K at the molar ratio of 50:10:38.5:1.5 were dispersed in absolute ethanol, shaken well, and stored at 4 °C. Next, 1 mg of mRNA was added to sodium acetate buffer, and then the organic phase mixture and mRNA-sodium acetate solution were added to the two inlets of the INano™ L nanomedicine preparation system in a volumetric ratio of 3:1. Liposomal
nanoparticles were prepared at a flow rate of 12 mL/min. After ultrafiltration and solution exchange, the LNP-encapsulated mRNA was dispersed in 10× PBS. Particle size was characterized using a Zetasizer Nano ZS to obtain the average particle size and the polydispersity index (P1). The product was then diluted or concentrated to obtain the required concentrations, and aliquots of the solution were stored at 4 °C.

**In vivo mRNA expression**

Female BALB/c mice (6–8 weeks old) (Beijing Vital River Laboratory Animal Technology Co., Ltd., Beijing, China) were randomly divided into six groups (n = 3 per group). Mice were intravenously administered with 150 μg of the original AET2010 or one of the mRNA-LNPs; blank LNPs served as the negative control group. Mouse serum samples were collected at 2, 6, 12, 24, 48, 72, and 96 h after administration of treatment and stored at −80 °C for subsequent testing. Serum antibody concentration was assessed using ELISA, as described above. The animal use protocol was approved by the Animal Ethics Committee of the Academy of Military Medical Sciences (No. IACUC-DWZX-2021-032).

**Statistical analysis**

In animal experiments, all data were presented as mean ± standard deviation (SD), and statistical analyses were performed using GraphPad Prism software (version 8.0). The differences between the groups were analyzed by a two-tailed Student’s t-test and considered statistically significant if p < 0.05 (**p < 0.01, ***p < 0.001). The quantitated concentrations of AET2010 were presented as mean ± SD and the data were analyzed using GraphPad Prism software.

**Results**

**AET2010 showed therapeutic potential for cancer in TIGIT-humanized BALB/c mice**

We synthesized AET2010 and two control antibodies RG6058 and MK7684 and studied the binding activity of the three antibodies to TIGIT using a surface plasmon resonance assay. Compared with the two control antibodies, AET2010 showed a weaker affinity of 2.92 nM (Figure 1A-1C), which was consistent with our previous findings [21]. Next, we established a xenograft tumor model in TIGIT-humanized BALB/c mice with subcutaneous inoculation of CT26 colorectal cancer cells and assessed the anti-tumor efficacy of the antibodies. The results (Figure 1D) showed that AET2010 displayed significant tumor proliferation inhibitory activity with a TGI rate of 50.19%, which was slightly lower than that of RG6058 (69.41%) and MK7684 (62.67%), but there was no significant difference observed between anti-TIGIT antibody groups. Thus, the therapeutic potential of AET2010 for cancer was further confirmed using a precise and favorable model.
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Figure 1: Representative sensorgrams of AET2010 (A), RG6058 (B), and MK7684 (C) interacting with human TIGIT in surface plasmon resonance assays and their anti-tumor efficacy in TIGIT-humanized BALB/c-hTIGIT mice (D, E). The antibodies were immobilized on the sensor chip surface, and human TIGIT-His at serially diluted concentrations was passed over the chip. The fitting curves (thin black lines) were derived from the analysis using the 1:1 binding mode. Equilibrium dissociation constants ($K_D$) were calculated according to the fitting curves. $K_D = k_d / k_a$; $k_a$, association rate constant; $k_d$, dissociation rate constant. (A) AET2010, $K_D = 2.92$ nM; (B) RG6058, $K_D = 0.27$ nM; (C) MK7684, $K_D = 0.146$ nM. Changes in tumor volume (D) and body weight (E) signifying the anti-tumor efficacy of antibodies in BALB/c-hTIGIT mice subcutaneously inoculated with CT26 cells. TGI, tumor growth inhibition; mpk, milligram per kilogram; BIW, twice a week; i.p., intraperitoneal injection. Data were analyzed using GraphPad Prism Software, and data are presented as mean ± standard deviation. *** $p < 0.001$, ** $p < 0.01$, * $p < 0.05$ (unpaired $t$-test); $n = 6$.

Figure 2: Design and optimization of mRNAs encoding AET2010. Cap 1 was selected as the cap structure for both types of mRNAs; the poly-A tail was added to the mRNA tail by polymerase after the DNA was transcribed into mRNA. (A) The encoding region of light and heavy chains was contained in a single ORF (mRNA-S). The 5' UTR was derived from human α-globin RNA with an optimized Kozak sequence, and the 3' UTR contained two sequence elements derived from the partial amino-terminal enhancer of split (AES) mRNA and the mitochondrial-encoded 12S ribosomal RNA. The encoding region of light and heavy chains was separated by the 2A "self-cleaving" peptides (P2A) gene. (B) The encoding region of light and heavy chains was contained in two separate ORFs (mRNA-B), and the 5' UTR and 3' UTR sequences matched those of mRNA-S. (C-E) Optimized mRNAs based on mRNA-B. (C) The codons of the light chain and heavy chain were optimized (mRNA-BC). (D) The 5' UTR was substituted with UTR2 with high ribosome loading derived from the NCBI Gene Expression Omnibus database (the original library ID of UTR2: 317915), and the 3' UTR was replaced by two copies of human β-globin mRNA (HBB gene) in tandem (mRNA-BU). (E) Both codon optimization and UTR substitution were performed (mRNA-BCU).
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Figure 3: Preparation and in vitro expression of mRNAs. (A) Agarose gel electrophoresis of prepared mRNA-S (Lane 3), the heavy chain of mRNA-B (Lane 1), and the light chain of mRNA-B (Lane 2). Lane M: single-stranded RNA (ssRNA) ladder. (B) Agarose gel electrophoresis of optimized mRNAs. Lane M: ssRNA ladder, 1: the heavy chain of mRNA-B, 2: the light chain of mRNA-B, 3: the heavy chain of mRNA-BC, 4: the light chain of mRNA-BC, 5: the heavy chain of mRNA-BU, 6: the light chain of mRNA-BU, 7: the heavy chain of mRNA-BCU, and 8: the light chain of mRNA-BCU. (C) In vitro expression levels of AET2010 by synthesized mRNAs transfected into CHO, COS-7, and HEK-293 cells. CHO, Chinese Hamster Ovary cells; COS-7, African green monkey SV40 transformed kidney cell; HEK-293, Human embryonic kidney 293 cells.

Figure 4: Distribution of codon usage bias of mRNA-B open reading frame sequence by MinMax% before (left panel) and after (right panel) codon optimization. The horizontal axis shows the amino acid sequence number of the heavy chain and light chain, respectively. Min% represents the proportion of rare codons; Max% represents the proportion of favorable codons.

Notably, UTR substitution or codon optimization alone significantly improved the expression levels of mRNA-B but not simultaneous optimization, which may have resulted from the synergism of the mRNA structural elements.

Table 1: MFE, GC% and CAI values of the open reading frame sequence of mRNA-B before and after codon optimization.

<table>
<thead>
<tr>
<th>Sequence</th>
<th>MFE</th>
<th>GC%</th>
<th>CAI</th>
</tr>
</thead>
<tbody>
<tr>
<td>Before optimization</td>
<td>-835.4</td>
<td>0.582</td>
<td>0.773</td>
</tr>
<tr>
<td>After optimization</td>
<td>-744.4</td>
<td>0.612</td>
<td>0.938</td>
</tr>
</tbody>
</table>

MFE is the minimum free energy; the smaller the MFE, the more stable the mRNA. GC% is the ratio of guanine to cytosine; the higher the GC content, the more stable the mRNA. CAI, codon adaptation index; the CAI values range from 0 to 1, and the greater the value, the stronger the fitness.

We prepared the optimized mRNAs (Figure 3B) and investigated their in vitro expression (Figure 3C). The expression efficiency of mRNA-BC and mRNA-BU was significantly higher than that of mRNA-B, whereas the optimization of mRNA-BCU did not have a significant effect.

Notably, UTR substitution or codon optimization alone significantly improved the expression levels of mRNA-B but not simultaneous optimization, which may have resulted from the synergism of the mRNA structural elements.

Furthermore, we injected 150 μg of LNP-encapsulated mRNA into mice via the caudal vein to investigate the in vivo expression efficiency and pharmacokinetic characteristics, and mice challenged with an equivalent dose of the original AET2010 were used as a control. The peak concentrations of AET2010 expressed by LNP-encapsulated mRNAs in mice were significantly higher than that obtained with the original AET2010, and the high concentrations were maintained for a longer duration (Figure 5). Among the mRNAs, mRNA-BU displayed the highest expression efficacy of AET2010 and reached a peak concentration of 581.308 μg/mL at 24 h.
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Figure S1: Predicted secondary structures of designed mRNAs. The outcome was made by LinearDesign Web Server (beta) (http://rna.baidu.com/). Nucleotides are assigned a color according to their position in the molecule. Lower-numbered nucleotides are closer to the 5' end and are colored green. Nucleotides in the middle are colored yellow, whereas nucleotides near the 3' end are colored red. Nucleotides are colored according to the type of structure that they are in: green, stems (canonical helices); red, multiloops (junctions); yellow, interior loops; blue, hairpin loops; orange, 5' and 3' unpaired regions. (A) The heavy chain of mRNA-B (MFE = -629.2 kcal/mol); (B) the light chain of mRNA-B (MFE = -399.6 kcal/mol); (C) the heavy chain of mRNA-BC (MFE = -597.1 kcal/mol); (D) the light chain of mRNA-BC (MFE = -347.8 kcal/mol); (E) the heavy chain of mRNA-BU (MFE = -623.0 kcal/mol); (F) the light chain of mRNA-BU (MFE = -378.1 kcal/mol); (G) the heavy chain of mRNA-BCU (MFE = -582.7 kcal/mol); and (H) the light chain of mRNA-BCU (MFE = -346.1 kcal/mol).

Figure 5: In vivo expression of AET2010 by lipid nanoparticle (LNP)-encapsulated mRNAs in mice. The mRNAs were packaged into LNPs using the INano™ L nanomedicine preparation system. Mice were intravenously injected with 150 μg of the original AET2010 or the mRNA-LNPs. Serum samples were collected at 2, 6, 12, 24, 48, 72, and 96 h post-administration, and the serum concentration of AET2010 was determined using enzyme-linked immunosorbent assay with recombinant TIGIT.
Discussion

TIGIT is a potential target for tumor immunotherapy, and the anti-tumor efficacy of TIGIT blockade may result from the killing effect of NK and T cells on tumor cells. We obtained a candidate anti-TIGIT antibody AET2010 in a previous study and demonstrated its anti-tumor efficacy in a xenograft mouse model with an adoptive transfer of NK-92MI cells. However, the limitations of that model made it necessary to further confirm the efficacy of AET2010. As an important assessment tool for tumor immunotherapy, target-humanized mice can fully simulate target-related effector cells and be used to efficiently predict the pharmacodynamics of candidate drugs. In the present study, we used TIGIT-humanized BALB/c mice, constructed a xenograft tumor model with subcutaneous inoculation of CT26 cells, and ultimately verified the significant anti-tumor efficacy of AET2010 with a TGI rate of 50.19% (Figure 1D). This result underpinned the potential of AET2010 as a therapeutic candidate.

Theoretically, mRNAs synthesized in vitro can utilize human cells as bioreactors to produce any protein drug in vivo, which also provides a novel avenue to antibody therapy [1,28]. In cancer immunotherapy, although there are few reports about antibody-encoding mRNAs, it is still worth expecting their long-term persistence and the subsequent durable anti-tumor immune response with a low frequency and dose of administration of antibody-encoding mRNAs. In the present study, we further explored the design and optimization of mRNAs encoding AET2010. First, we designed two types of mRNAs expressing AET2010, that is, the sequences encoding the light and heavy chains of the antibody were situated in one or two ORFs (mRNA-S or mRNA-B) and confirmed the high expression efficiency of mRNA-B (Figure 3C). The poor expression efficiency of mRNA-S is most likely explained by its ultralong sequence. Simultaneously, we attempted to synthesize circular mRNAs encoding the heavy chain and light chain of AET2010 separately, but the circularization efficiency was too low to achieve success (data not shown). Furthermore, based on mRNA-B, we revealed that the optimization by UTR substitution (mRNA-BU) significantly improved the in vitro and in vivo expression efficiency of AET2010 (Figure 3C and Figure 5). However, the codon usage bias optimization alone (mRNA-BCU) or its combination with UTR substitution (mRNA-BCU) did not lead to significant improvement in the in vitro or in vivo expression, which may have resulted from the structures of mRNAs and their LNP encapsulation. Notably, durable expression of active AET2010 in high concentrations was observed following in vivo administration of mRNAs, which signifies that AET2010-encoding mRNAs have a potential application value. In addition, further studies need to investigate whether circular mRNAs or self-replicating mRNAs encoding AET2010 have higher expression efficiency. Based on the present findings, we plan to further investigate the strong pharmacodynamic effects of AET2010-encoding mRNAs with reduced administration frequency and dose, especially mRNA-BU.

Conclusion

In summary, we confirmed the anti-tumor efficacy of the candidate anti-TIGIT antibody AET2010 and obtained a candidate mRNA that efficiently encodes active AET2010 in vivo (mRNA-BU), which provides a basis for the development of novel drugs targeting TIGIT.

Author contributions

Conceptualization, P.D. and J.C.; Methodology, J.C., G.Q., and X.W.; Software, J.C.; Formal analysis, J.C., P.D., and G.Q.; Investigation, J.C. and G.Q.; Resources, J.C. and G.Q.; Data curation, J.C.; Writing—original draft preparation, J.C., G.Q., and P.D.; Writing—review and editing, Y.C., Z.Y., J.C., F.L., H.Q., and P.D.; Supervision, P.D., Y.C., Z.Y., and F.L.; Project administration, Y.C., Z.Y., P.D., and J.C. All authors have read and agreed to the submitted version of the manuscript.

Data availability statement

The datasets generated during and/or analyzed during the current study are available from the corresponding author upon reasonable request.

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